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## Introduction

- The extracellular matrix (ECM) is an essential part of the cellular microenvironment and conveys both chemical and mechanical cues that play a significant role in regulating cellular behavior<sup>1,2,3</sup>.
- Biomechanical properties of the ECM, such as stiffness and porosity, are known to dictate the forces exerted by cells onto their surroundings and influence cellular function in complex, three-dimensional (3D) environments *in vivo*<sup>1,2,3</sup>.
- Light-based stiffness modulation can be achieved using a photosensitizer (PS), a molecule that absorbs visible light and reaches an excited triplet state<sup>2,4</sup>.
- This longer-lived triplet state of a PS produces reactive species such as singlet oxygen that fuel the necessary biomolecular reactions to either increase or decrease stiffness depending on the type of PS and its corresponding excitation wavelength<sup>2,4</sup>.

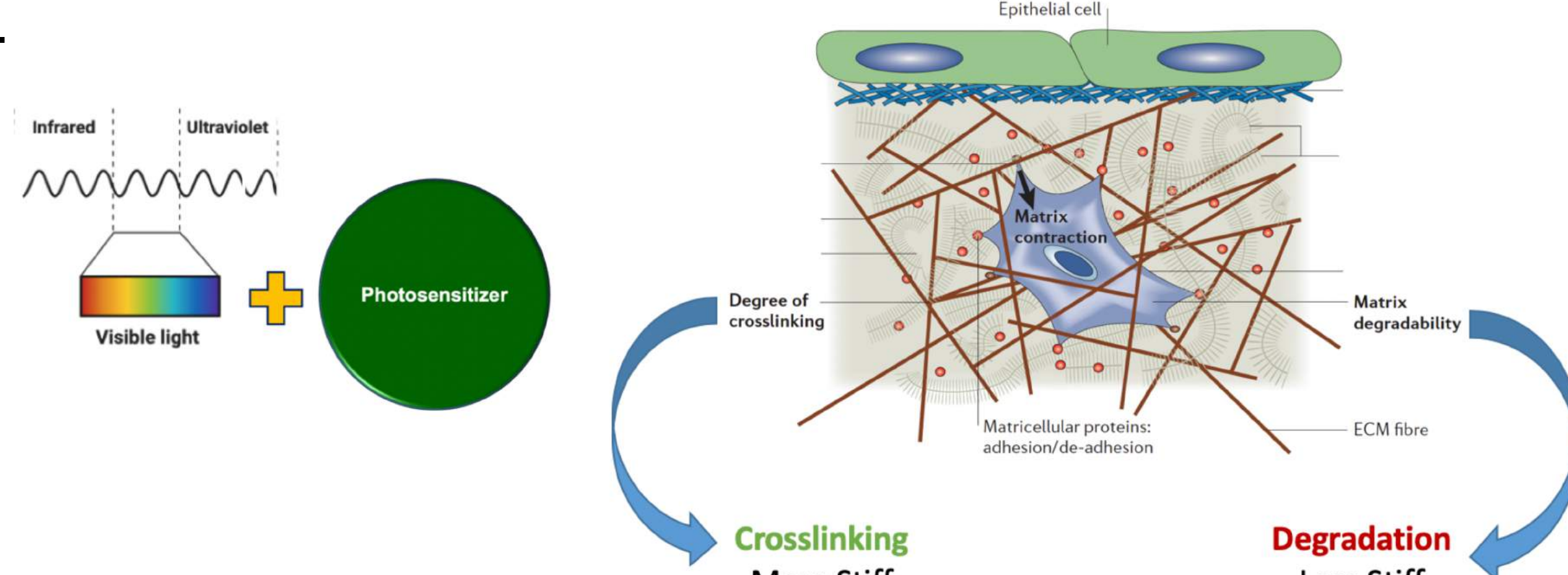


Figure 1<sup>3</sup>. Altering the mechanical properties of the cellular microenvironment using photochemistry

**Aim 1:** Quantify the effects of benzoporphyrin derivative (BPD)-mediated photodegradation and riboflavin-mediated photocrosslinking on the stiffness of Matrigel hydrogels using nanoindentation.

**Aim 2:** Develop a photomask prototype to serve as a preliminary optical patterning platform.

## Methods

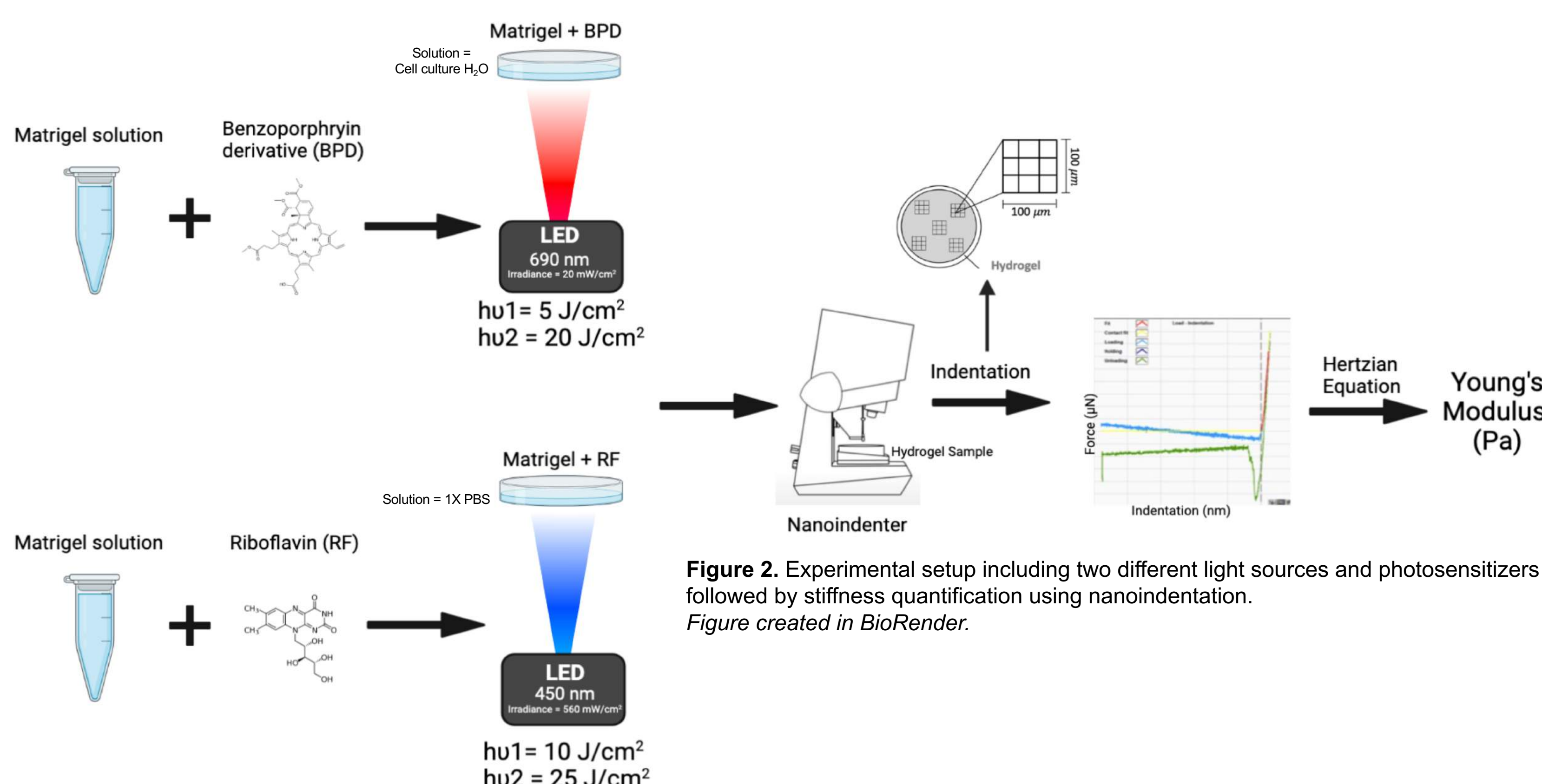
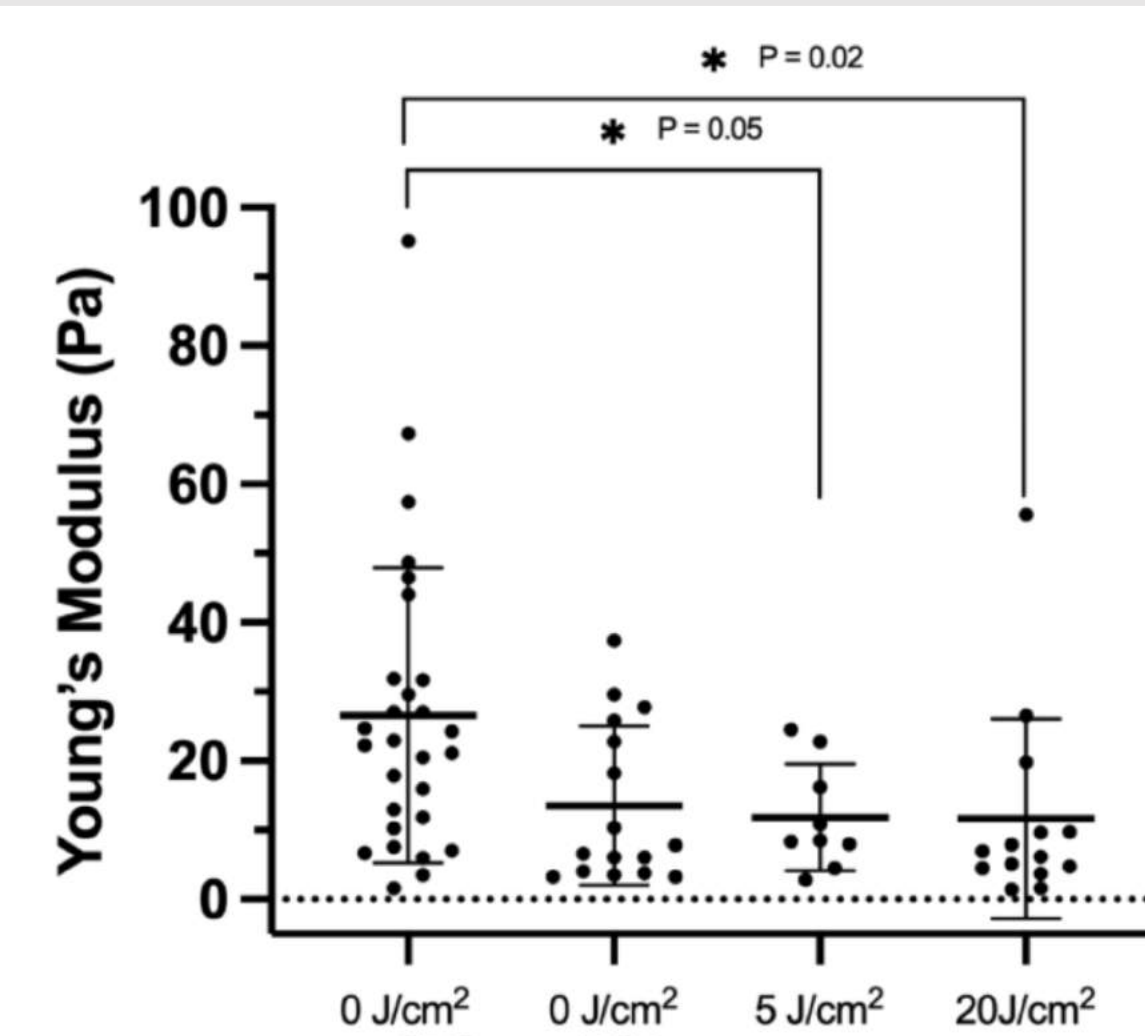


Figure 2. Experimental setup including two different light sources and photosensitizers followed by stiffness quantification using nanoindentation. Figure created in BioRender.

- For experiments with BPD, the final concentration of PS was **250 nM** and Matrigel hydrogels were incubated for **45 minutes** before irradiation and nanoindentation.
- For experiments with RF, the final concentration of PS was **0.1%** and Matrigel hydrogels were incubated for **24 hours** before irradiation and nanoindentation using a heated stage.
- Force curves were analyzed with Piuma Dataviewer V2.3 software.

## Results



### BPD-mediated Photodegradation

Gel Condition	Number of Curves Fit/Total Curves*	Mean (Pa)	SD
60% Matrigel No BPD no hv	28/45	26.56	21.30
60% Matrigel BPD no hv	16/45	13.52	11.52
60% Matrigel BPD hv1	9/45	11.83	7.712
60% Matrigel BPD hv2	14/45	11.68	14.43

\*Curves fit using Hertz model and R<sup>2</sup> threshold of 0.8  
Figure 3. Distribution of stiffness measurements (recorded as Young's modulus) collected for each hydrogel. \* signifies p ≤ 0.05, according to an unpaired, two-tailed t-test.

- The lowest average stiffness recorded was 11.68 Pa when using red light (690 nm) at a light dose of 20 J/cm<sup>2</sup>.
- There was a significant difference (P ≤ 0.05) between the average stiffness of the control group that did not receive any light and or PS, and the two groups that received light doses of 5 J/cm<sup>2</sup> and 20 J/cm<sup>2</sup>.

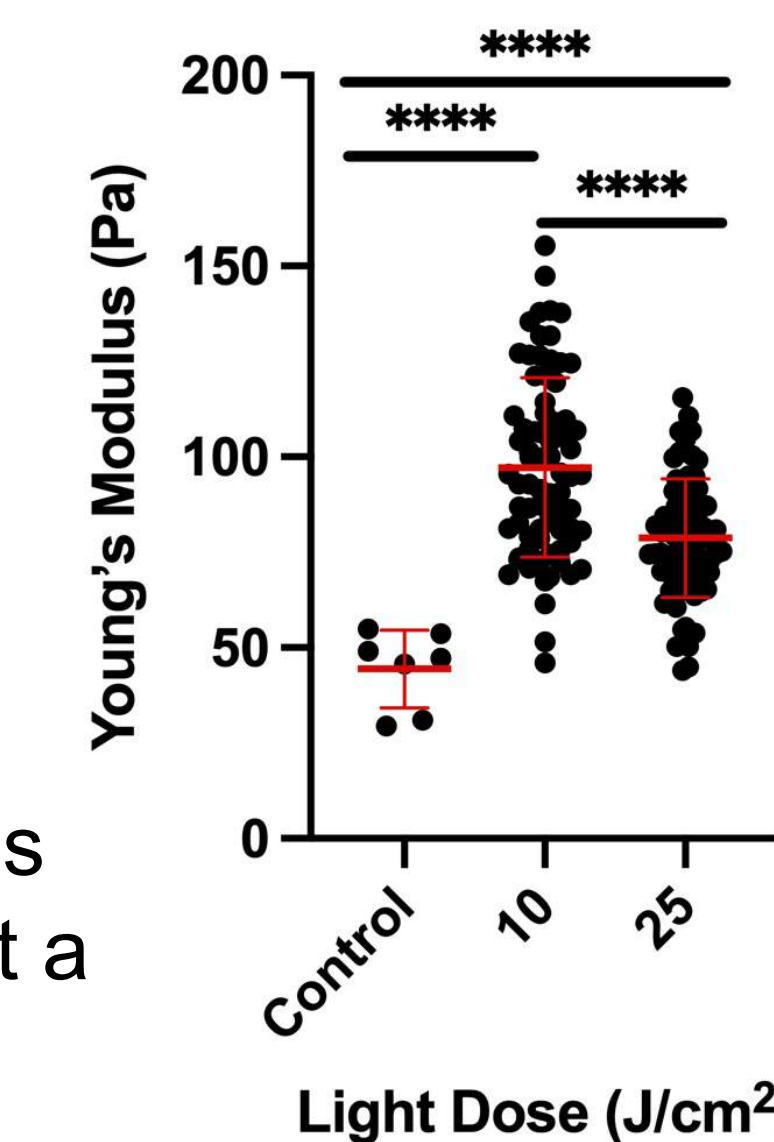


Figure 5. CAD drawing and 3D printed version of photomask platform.

### RF-mediated Photocrosslinking

Gel Condition	Number of Curves Above R <sup>2</sup> = 0.95	Mean (Pa)	SD
0 J/cm <sup>2</sup>	7/45	44.44	10.23
10 J/cm <sup>2</sup>	75/80	97.24	23.53
25 J/cm <sup>2</sup>	75/80	78.75	15.53

Figure 4. Distribution of stiffness measurements (recorded as Young's modulus) collected for each hydrogel. \*\*\*\* signifies p < 0.0001, according to an unpaired, two-tailed t-test.



- The highest average stiffness recorded was 97.24 Pa when using blue light (450 nm) at a light dose of 10 J/cm<sup>2</sup>
- Although there was a limited amount of stiffness measurements for the control group that received no light and no PS, there was a significant difference (P ≤ 0.05) between the average stiffness of the control and the two groups that received light doses of 10 J/cm<sup>2</sup> and 25 J/cm<sup>2</sup>.

- A photomask platform was developed using computer aided design software (OnShape) and 3D printed using a Stratasys printer
- The dimensions are 2.62 in x 2.62 in x 0.270 in and it is designed to fit a 35 mm glass bottom dish with a 10 mm microwell.

## Discussion and Conclusion

### BPD-mediated Photodegradation

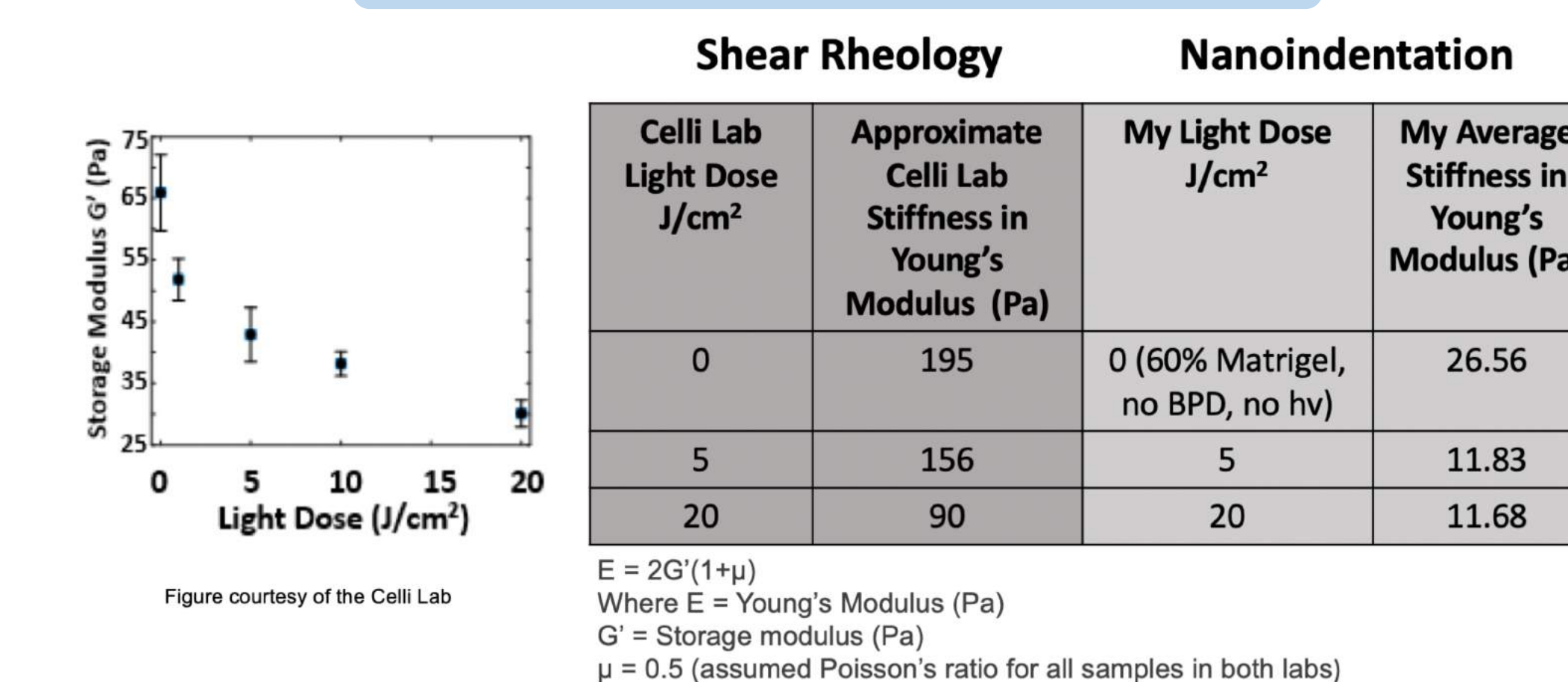


Figure 6. Comparison of stiffness measurements taken with a shear rheometer and a nanoindenter.

- The large standard deviations observed with BPD-mediated photodegradation (Fig. 3) indicate the nanoindenter's poor signal-to-noise ratio due to the compliance of the hydrogel.
- In comparison to stiffness measurements from the Celli Lab (Univ. of Massachusetts at Boston) taken with a shear rheometer, there was a consistent trend of decreasing stiffness for the same hydrogel and BPD concentration as light dose increased.
- The discrepancies between the average stiffness values (Fig. 6) is likely due to inherent differences in how the two instruments assess the mechanical properties of a hydrogel.

### RF-mediated Photocrosslinking

- Previous work reported stiffness values of approximately 420 and 465 Pa for collagen hydrogels irradiated at light doses of 10 and 25 J/cm<sup>2</sup>, respectively.
- The average stiffnesses reported here in Matrigel using the same light doses and riboflavin concentration are more compliant at 97.24 Pa and 78.75 Pa (Fig. 4).
- This difference may be dependent on the heterogenous composition of Matrigel and that it is comprised of only ~30% collagen, of which light-induced crosslinking effects such as stiffening are thought to result primarily from crosslinks in collagen<sup>4,5</sup>.

### Future Directions

- Quantify stiffness modulation in Type I collagen hydrogels after RF-mediated photocrosslinking at 450 nm and interrogate concurrent changes in porosity.
- Conduct preliminary optical patterning experiments and prototype improvements.

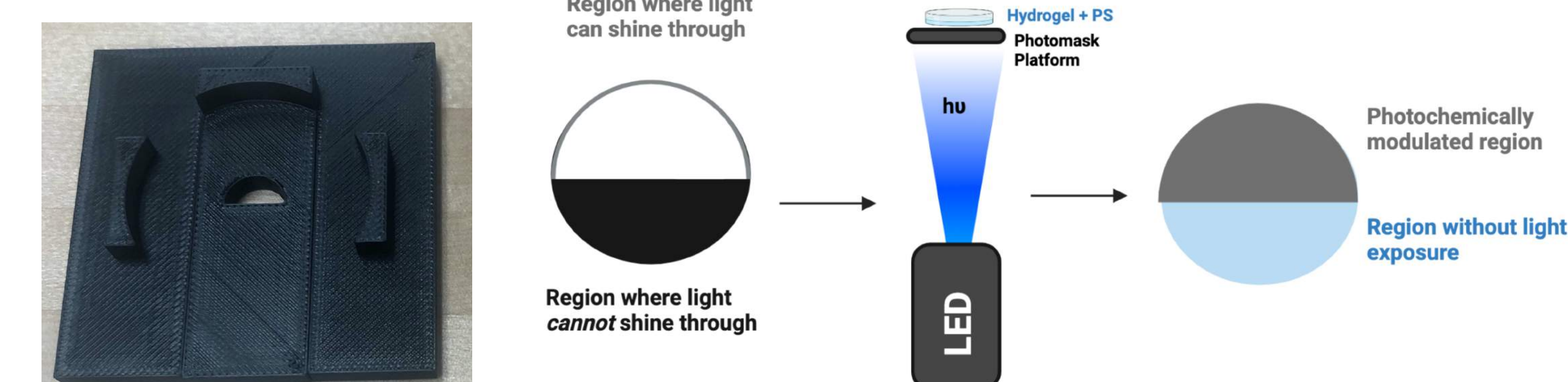


Figure 7. Experimental setup for future work with photochemistry-based optical patterning.